

# THEORETICAL STUDY OF MICROBUBBLE DYNAMICS UNDER THE ACTION OF ULTRASOUND FIELDS



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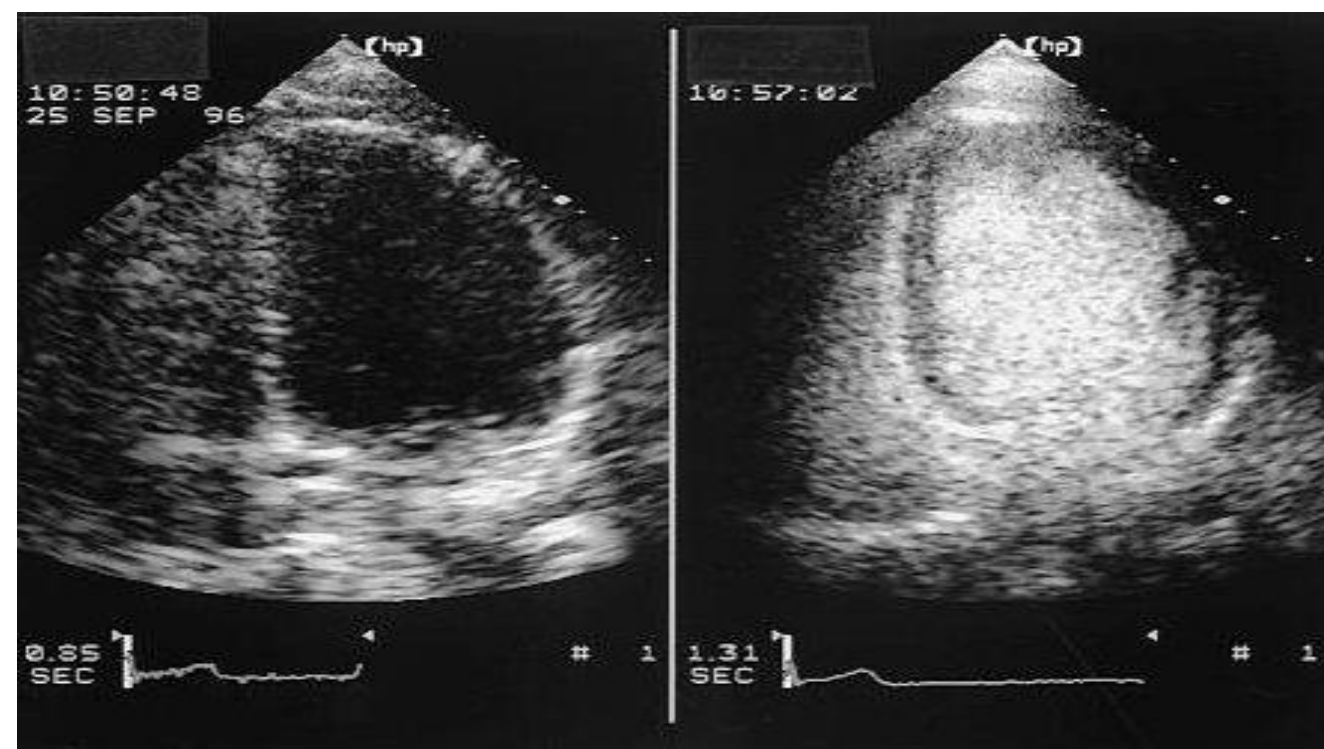
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## INTRODUCTION

Ultrasound contrast agents (UCAs) used to improve medical image. There are a lot of Contrast agents substance in the market which has different Parameters with different use for medical purposes. For that, there are a lot of models which describe the motion of bubble under the action of Ultrasound.

UCAs models are derived for the radius of the bubble as a function of time in response to a time dependent driving pressure. The most fundamental of the nonlinear models is a second order, ordinary differential equation, called the Rayleigh-Plesset (RP) equation.

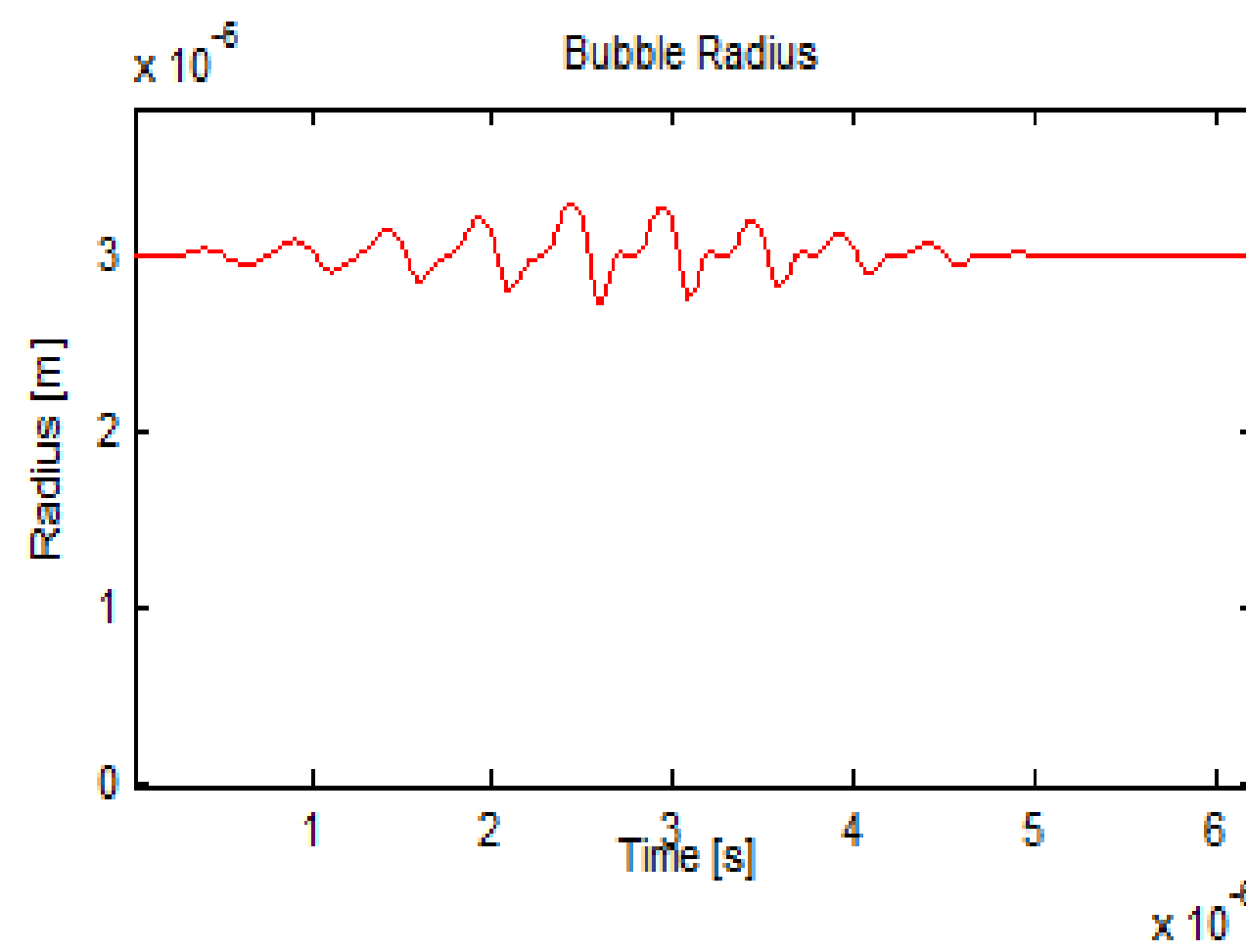
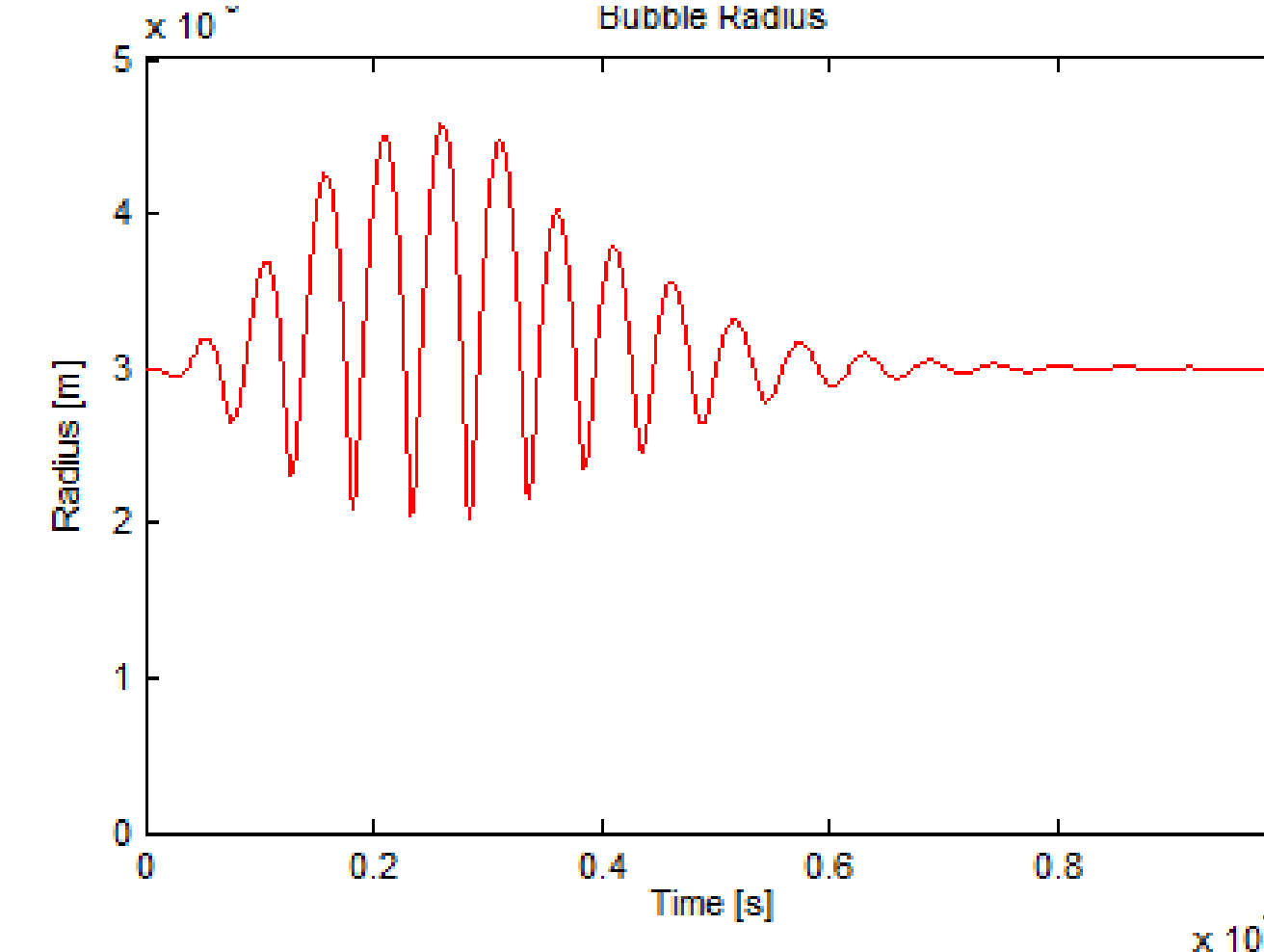


## ENCAPSULATING BUBBLE

### Hoff's Model

For Sonazoid®:

- Radius R0=3µm;
- pulse amplitude=0.3Mpa
- Pulse length 5 cycles
- frequency 2 MHz

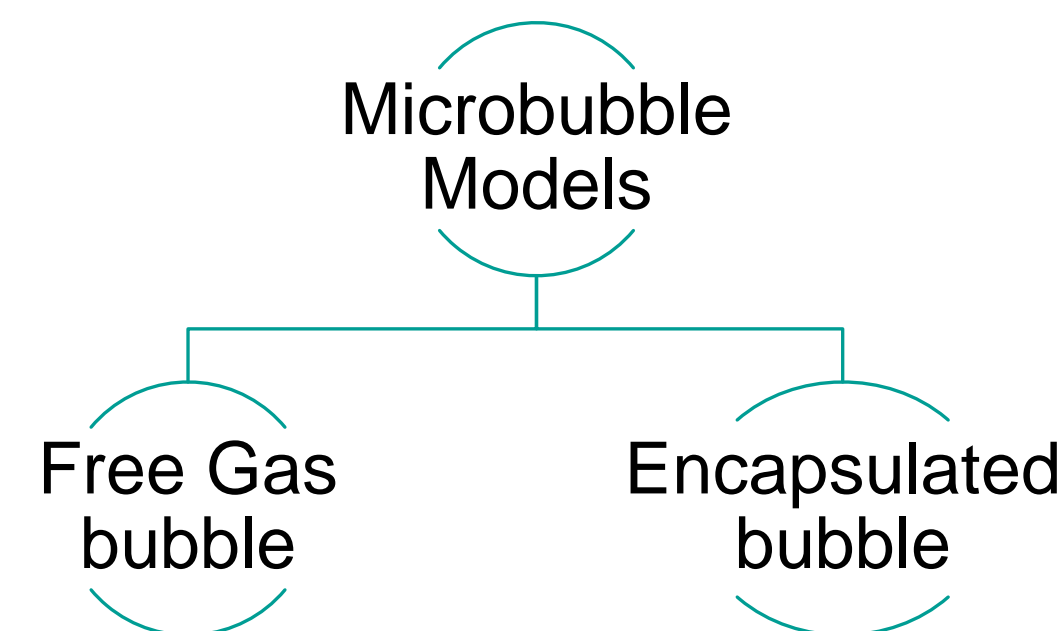


For Alunex®:

- Radius R0=15µm;
- pulse amplitude=0.3Mpa
- Pulse length 5 cycles
- frequency 2 MHz

Parameters and Values(Tab 2.3)		
Parameter	Value	Description
r		
p <sub>0</sub>	1.013 x 10 <sup>5</sup> Pa	Ambient pressure
ρ	1000 kg/m <sup>3</sup>	Density of liquid
γ	1.4	Polytropic exponent
Shell parameters		
Alunex®		
δ	15 nm	Shell thickness
G <sub>s</sub>	88,8 MPa	Shell elastic modulus
μ <sub>s</sub>	0,5 Pa s	Shell viscosity
Sonazoid®		
δ	4 nm	Shell thickness
G <sub>s</sub>	50 MPa	Shell elastic modulus
μ <sub>s</sub>	0.8 Pa s	Shell viscosity

## MODELS



Model for free gas bubble: **Rayleigh-Plesset Equation**

$$\rho \left( \ddot{R}R + \frac{3}{2} \dot{R}^2 \right) = p_0 \left( \frac{R_0}{R} \right)^{3\gamma} - p_0 - P(t)$$

Model for Encapsulating bubble:

- **Hoff's Model**

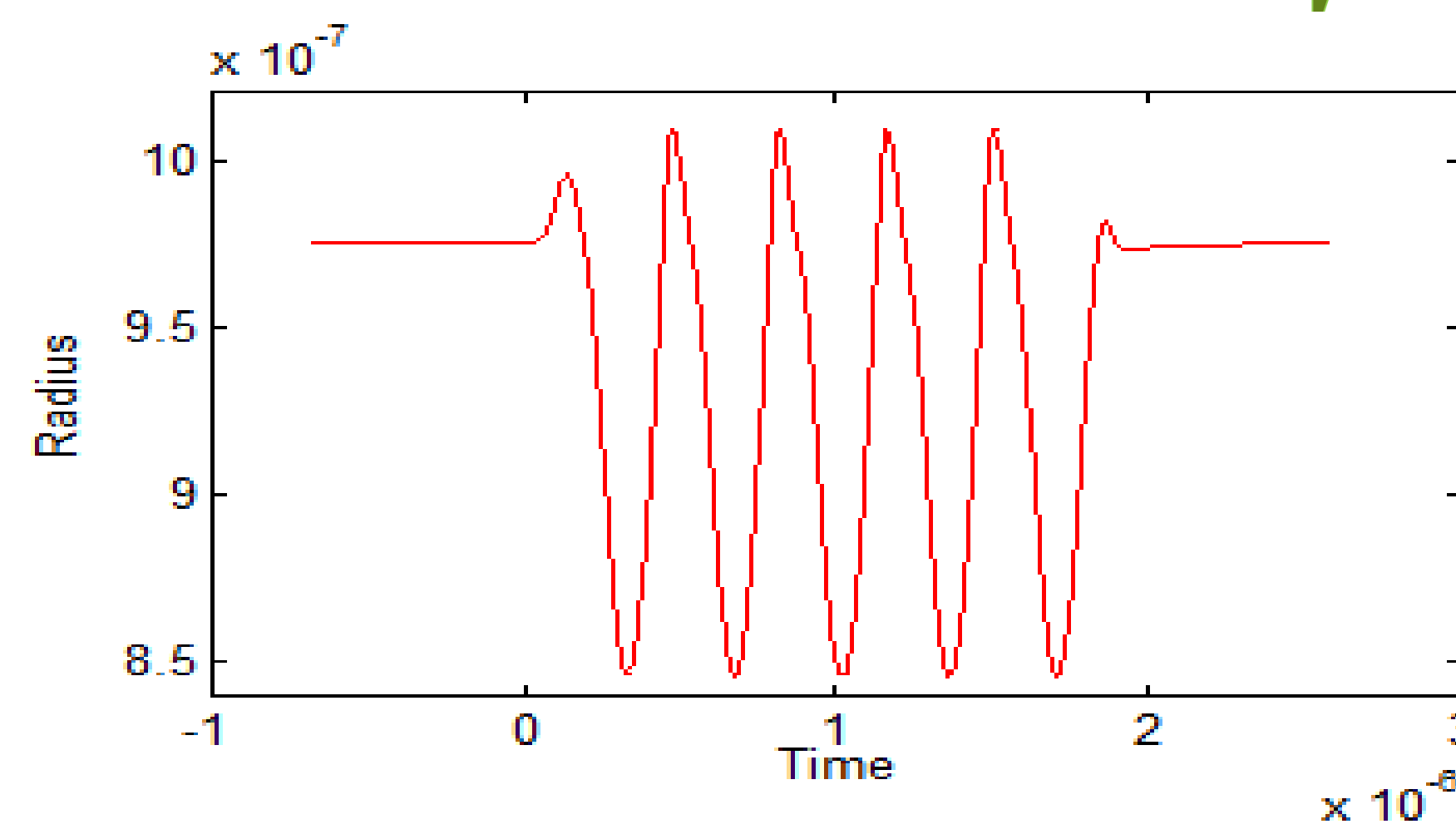
$$\rho_l \left( R\ddot{R} + \frac{3}{2} \dot{R}^2 \right) = p_0 \left( \left( \frac{R_0}{R} \right)^{3k} - 1 \right) - P(t) - 4\mu_l \frac{\dot{R}}{R} - 12\mu_s \frac{d_{s,0} R_0^2 \dot{R}}{R^3} - 12G_s \frac{d_{s,0} R_0^2}{R^3} \left( 1 - \frac{R_0}{R} \right)$$

- **Marmottant's model**

$$\rho_l \left( R\ddot{R} + \frac{3}{2} \dot{R}^2 \right) = \left( p_0 + \frac{2\sigma(R_0)}{R_0} \right) \left( \frac{R_0}{R} \right)^{3k} \left( 1 - \frac{3k}{c} \dot{R} \right) - p_0 - \frac{2\sigma(R_0)}{R} - 4\mu_l \frac{\dot{R}}{R} - \frac{4k_s \dot{R}}{R^2} - p(t)$$

Where **R** is the bubble Radius ,**P** is the pressure .

### Marmottant's Model

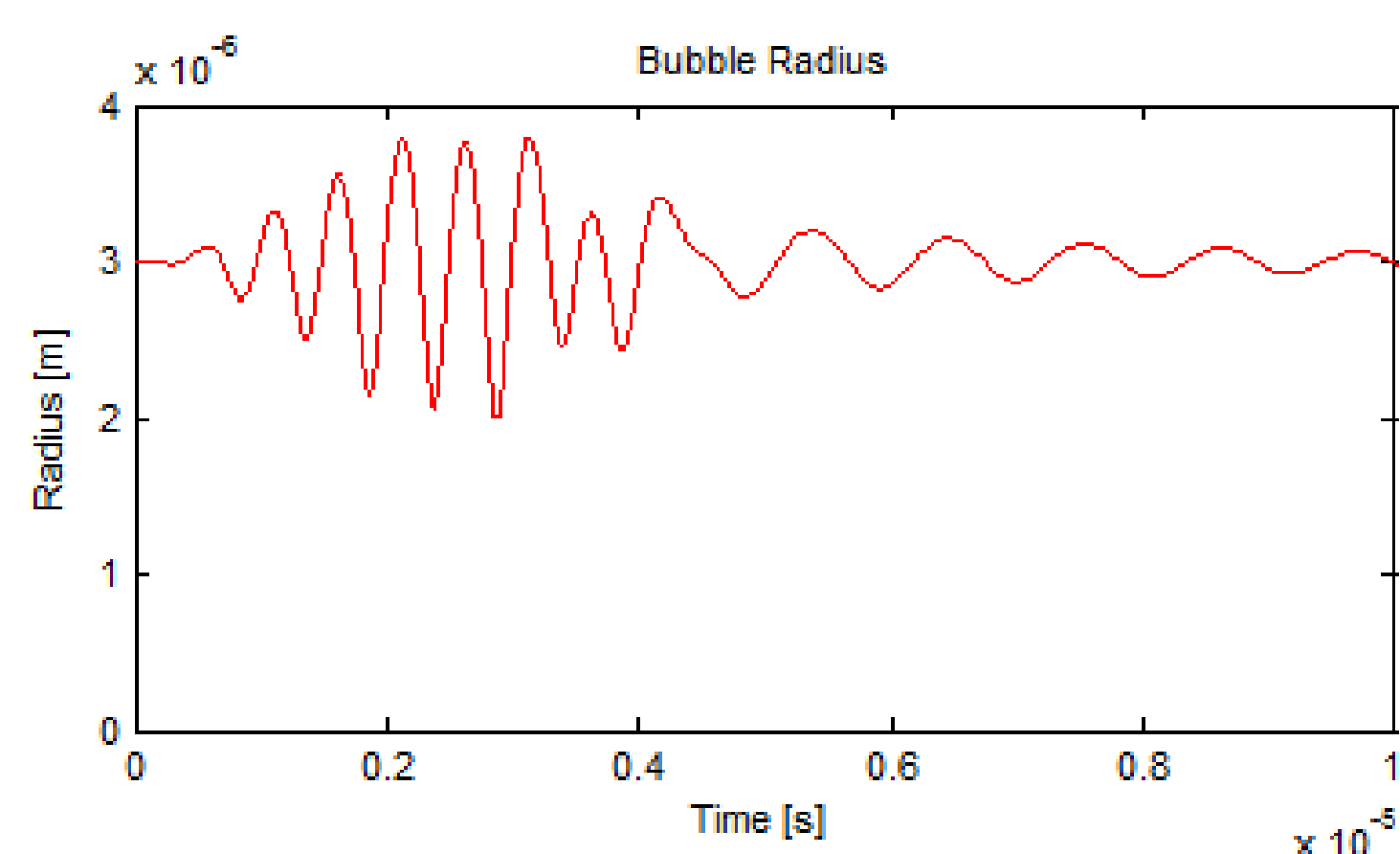


- Radius Buckling R<sub>0</sub>=0.975 µm
- χ=1 N/m; k<sub>s</sub>=15x10<sup>-9</sup> N
- σ<sub>break up</sub>>1 N/m
- frequency 2.9 MHz

## FREE GAS BUBBLE

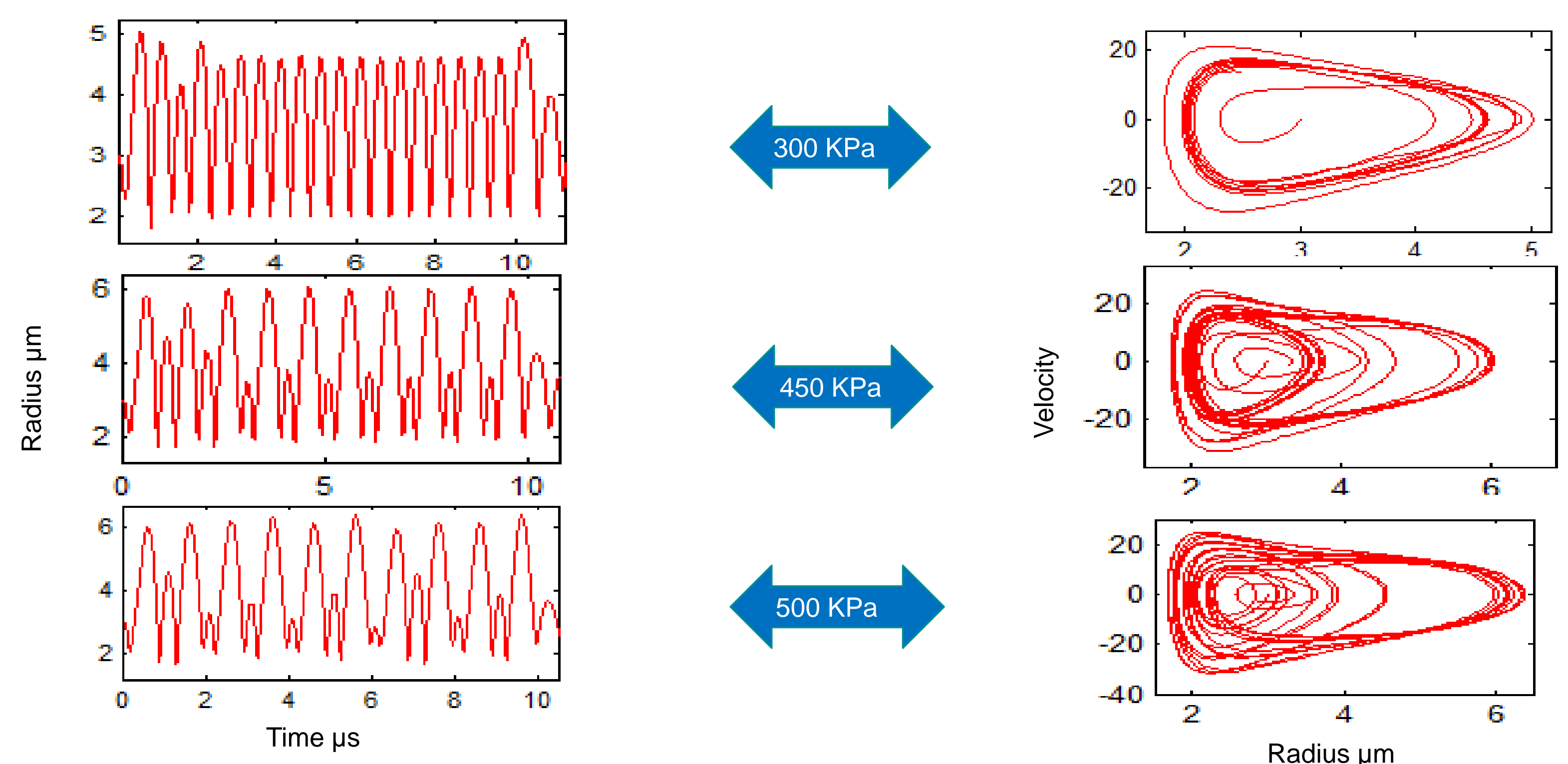
### Rayleigh-Plesset Equation

With center frequency 2 MHz and using water as liquid, Bubble response will be:



## NONLINEAR BEHAVIOR

- The bubble behaves as a nonlinear oscillator at high amplitude
- With increasing the pulse amplitude with increasing Chaotic motion



## CONCLUSIONS

- Hoff model depends on viscoelastic parameters of the shell material.
- Marmottant depend on surface tension (buckling radius, a shell compressibility, and a break-up shell).
- The fundamental assumptions of the models, such as spherically symmetric and stationary bubbles are unrealistic for contrast agents in the body.

